

# *In vivo* Hyperpolarized $^{13}\text{C}$ Chemical Shift Imaging using Variable Flip Angle and Centric Phase Encoding of Stimulated Mouse Muscle

Tangi Roussel, Avigdor Leftin and Lucio Frydman  
Department of Chemical Physics, Weizmann Institute of Science, Israel

## Introduction

MR Spectroscopic Imaging (MRSI) of hyperpolarized  $^{13}\text{C}_1$ -pyruvate is a promising technique for *in vivo* mapping of metabolic information [1]. This method is based on **Dynamic Nuclear Polarization (DNP)** followed by a rapid dissolution process to produce a highly polarized metabolic contrast agent. After injection,  $^{13}\text{C}_1$ -pyruvate and its metabolic products  $^{13}\text{C}_1$ -lactate,  $^{13}\text{C}_1$ -alanine and  $^{13}\text{C}_1$ -bicarbonate can be mapped using a **Chemical Shift Imaging (CSI)** sequence. However, given the short life time of hyperpolarized signals, one of the main challenges of  $^{13}\text{C}$  hyperpolarized metabolic imaging remains the optimization of Signal-to-Noise Ratio (SNR) and of image quality [2]. In this study, a **Variable Flip Angle (VFA) Centric Phase Encoding (CPE) CSI** sequence was implemented and synchronized with a **multiple bolus** hyperpolarized  $^{13}\text{C}_1$ -pyruvate delivery strategy (Fig. 2) [3] to perform **real-time functional MRSI of skeletal muscle metabolism** during an exercise-mimicking nerve stimulation [4].

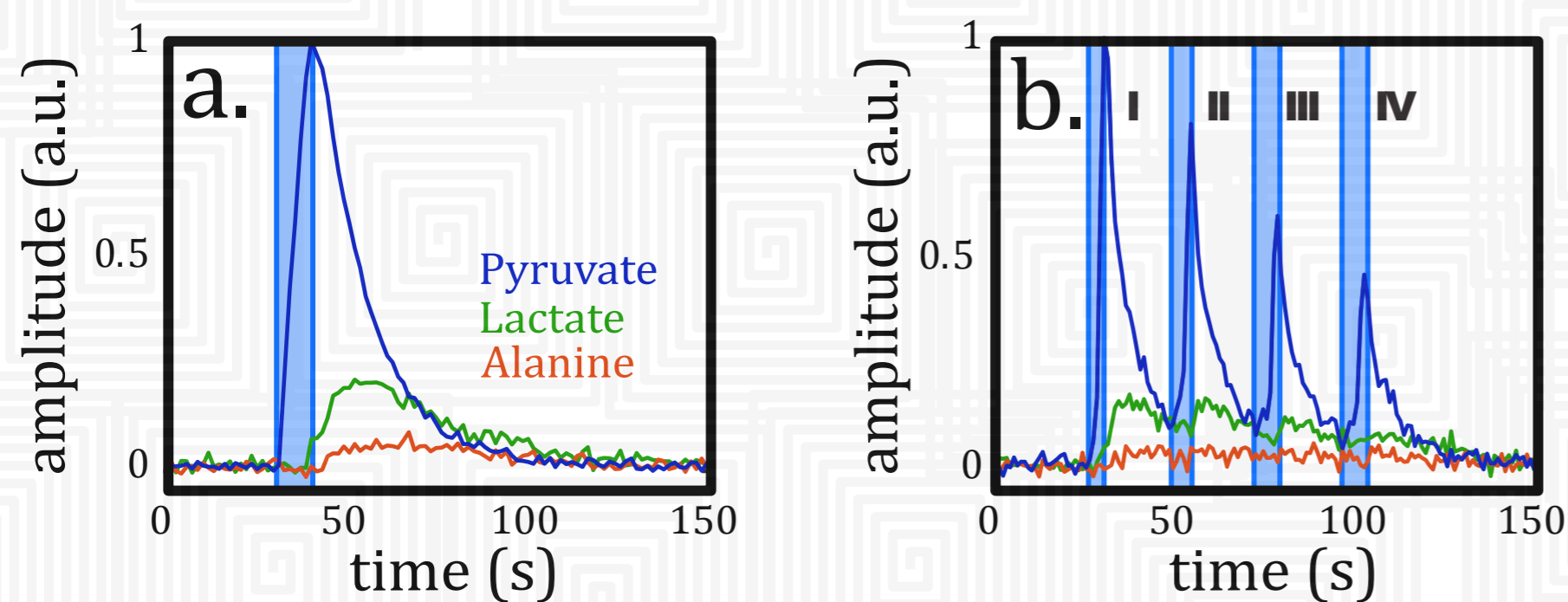


Fig. 2: *In vivo* (a) conventional and (b) multi-bolus tracer administration of  $^{13}\text{C}_1$ -pyruvate in mouse skeletal muscle.

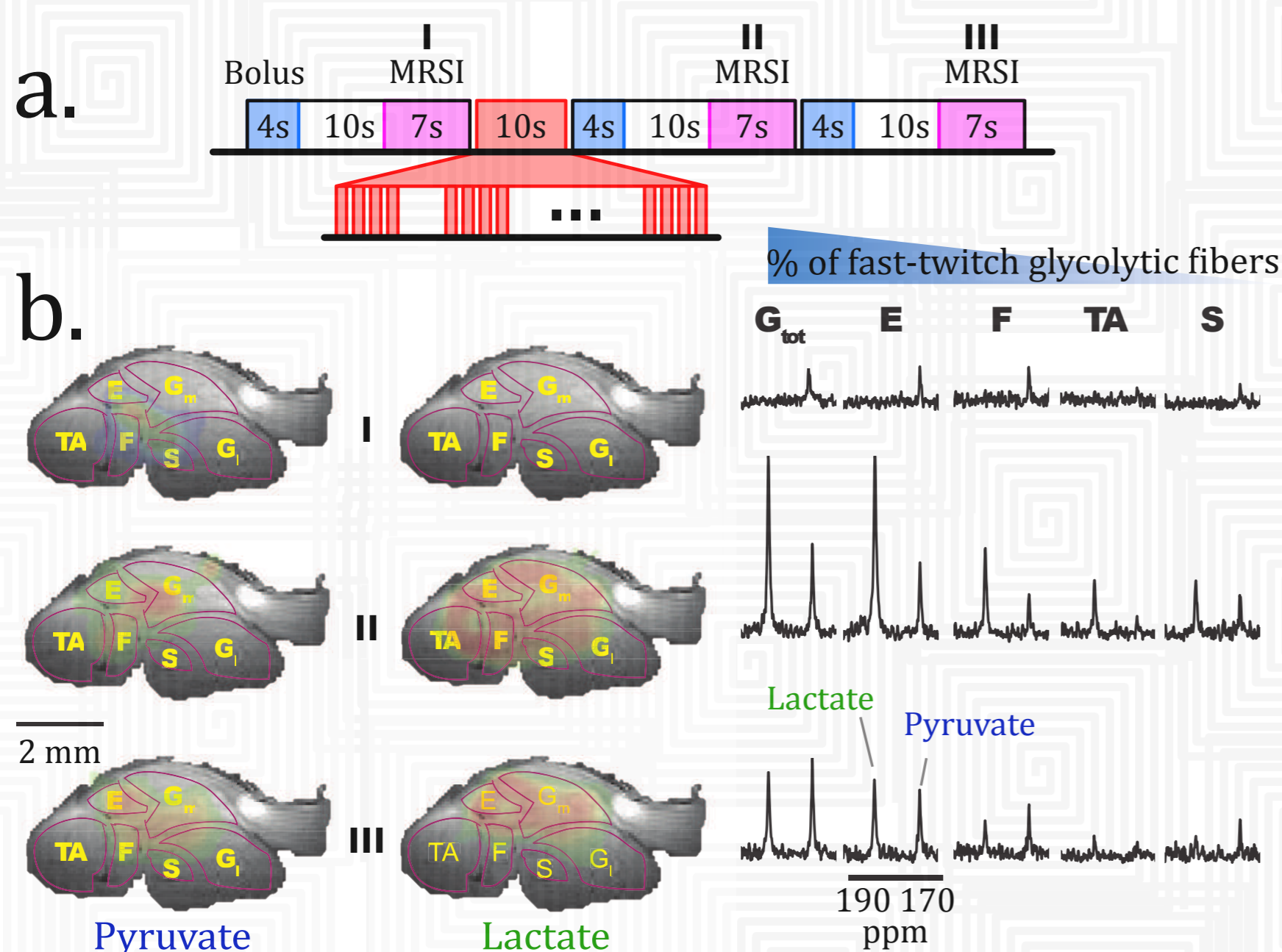


Fig. 3: Functional paradigm for hyperpolarized  $^{13}\text{C}_1$  magnetic resonance (a) and metabolite maps and spectra for  $^{13}\text{C}_1$  pyruvate and lactate (b).

## Results & Discussion

Metabolic functional MRS images were obtained from multiple bolus experiments using VA-CPE-CSI acquisitions are shown in Fig 3b. Pre-stimulation maps show only small amounts of  $^{13}\text{C}_1$  pyruvate, while **muscle stimulation causes rapid increases in SNR of the pyruvate tracer and increases its metabolism to  $^{13}\text{C}_1$ -lactate**, particularly in the fast-twitch glycolytic-rich gastrocnemius (G) muscle group.

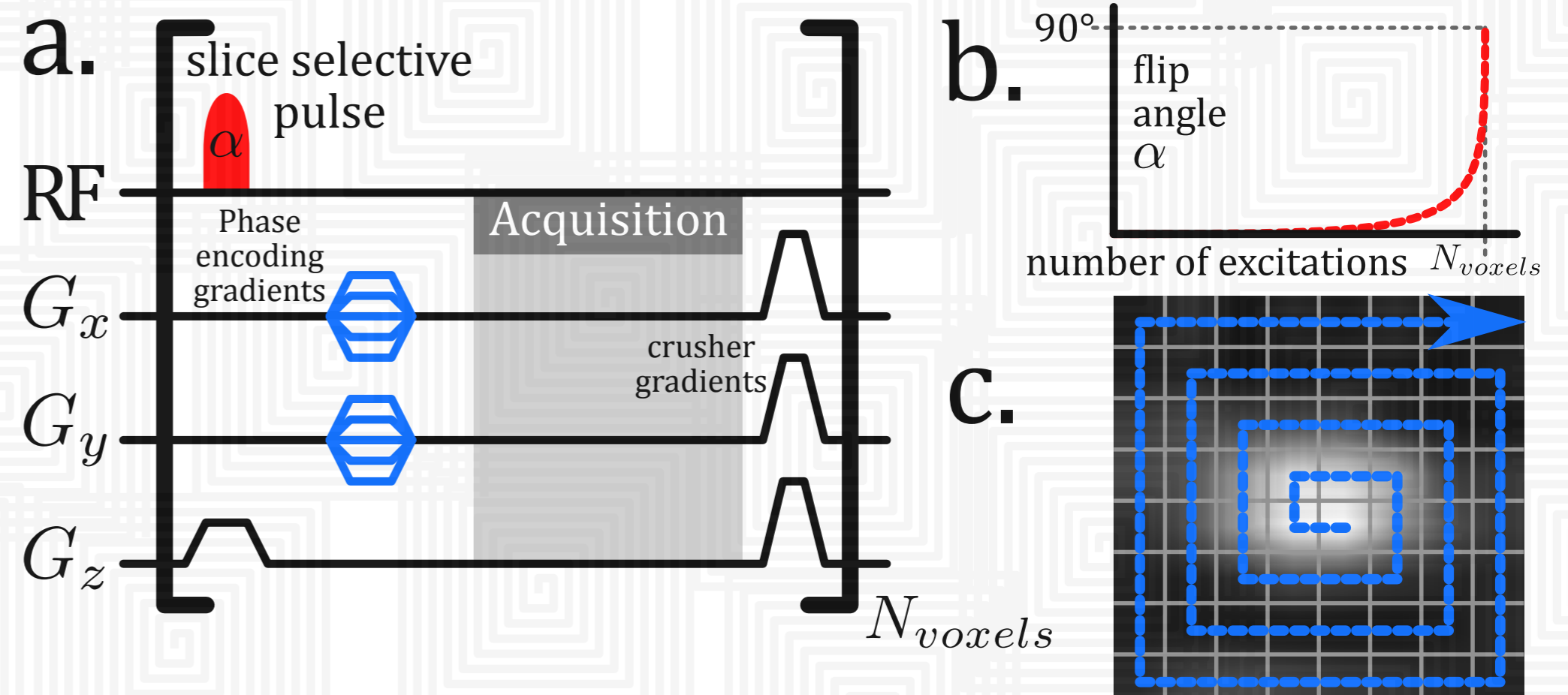


Fig. 1: Variable Flip Angle (VFA) - Centric Phase Encoding (CPE) - Chemical Shift Imaging (CSI) sequence (a), flip angle variation according the number of excitations (b) and CSI k-space filling (c).

## Method

**Pulse sequence.** The VFA-CPE-CSI sequence (Fig. 1a) was fully implemented on a Bruker Biospec 4.7T small animal imaging system equipped with a Doty Scientific 8mm transmit/receiver  $^1\text{H}/^{13}\text{C}$  surface coil.  $^1\text{H}$  MGE anatomic images were acquired using TE/TR=5.38ms/1s. The functional VFA-CPE-CSI acquisitions consisted of 64 phase encoding steps for an 8x8 in plane matrix (Fig. 1c) and a TR of 104ms, resulting in a total **scan time of 6.7s**. The CSI image FOV was 12.5mm x 12.5mm with a 2mm slice selection using a VFA Gaussian pulse (Fig. 1b). The CPE CSI data reconstruction was performed using a Matlab home-made procedure. The JRMUI software was used for data quantification with AMARES.

**Hyperpolarization.** A sample mixture of neat  $^{13}\text{C}_1$  pyruvic acid (Sigma) and OX-63 trityl radical (Oxford Instruments) was polarized on an Hypersense operating at 1.4K using microwave irradiation of 95GHz resulting in a 60mM hyperpolarized pyruvate sample was dissolved in pH 7.6 buffer and stored at 1T fringe field during the **injection of three boluses (133 $\mu\text{L}$  each)**, timed in synchrony with the external stimulus being imaged.

**Muscle Stimulation.** Female ICR mice (20 weeks old, 25g body weight) were anaesthetized by I.P. injection of sodium pentobarbital (70mg/kg). The sciatic nerve of the hind limb was surgically exposed, electrode leads fastened to the nerve and inserted in a foot pad, and sutured. The tail vein was catheterized for the hyperpolarized solutions injections. The animals were maintained anesthetized using isoflurane. **Electrical stimulation was performed using 10ms trains of positive 10V/200 $\mu\text{s}$  pulses repeated at 10Hz** (Fig. 3a). Data from each animal was collected using 4 experiments repeated under non-stimulated and stimulated conditions.

## Conclusion

VFA and CPE strategies implemented within the Bruker Paravision CSI method enabled the **acquisition of metabolic maps with high in-plane resolution for functional imaging of muscle metabolism using multiple boluses of hyperpolarized  $^{13}\text{C}_1$ -pyruvate**.

## References

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