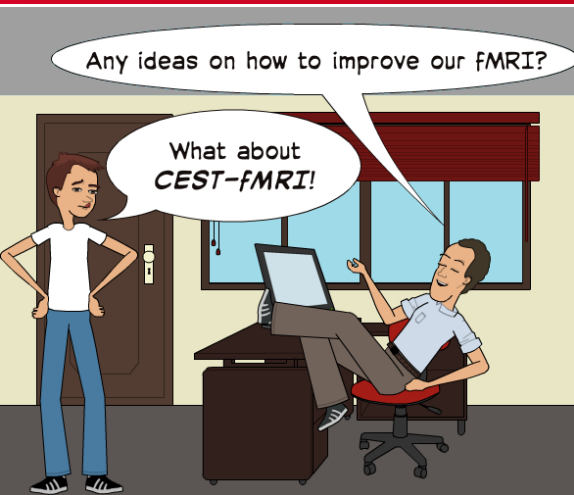


#247 - CEST fMRI at ultra-high magnetic field

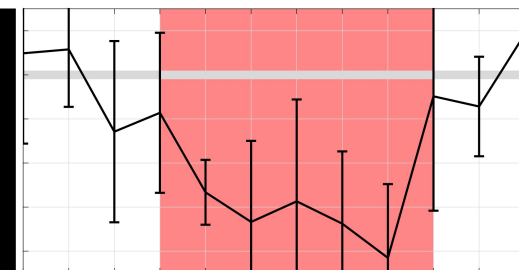
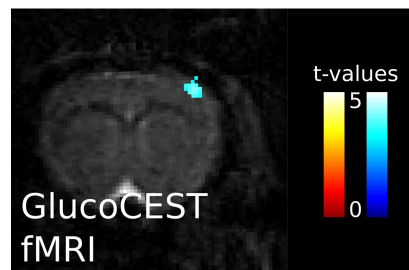
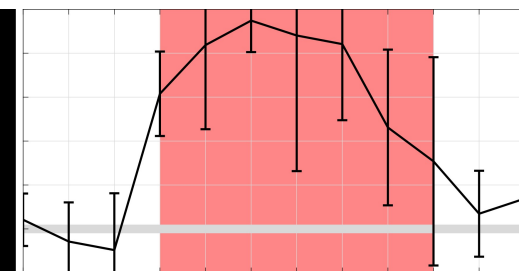
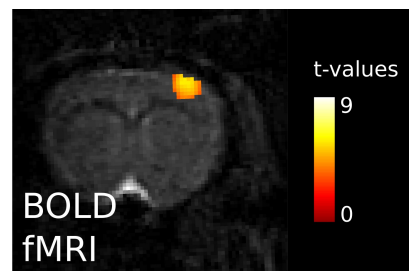
Plasma screen n°11



CEST = Chemical Exchange Saturation Transfer
+
Functional MRI at 17.2T

Novel fMRI contrast based on CEST!

→ GlucoCEST drop during activation



CEST fMRI at ultra-high magnetic field

Tangi Roussel¹, Lucio Frydman², Denis Le Bihan¹ and Luisa Ciobanu¹

[1] NeuroSpin, Commissariat à l'Energie Atomique et aux Energies Alternatives, Gif-sur-Yvette, France

[2] Department of Chemical Physics, Weizmann Institute of Science, 76100 Rehovot, Israel

DE LA RECHERCHE À L'INDUSTRIE



מכון ויצמן למדע
WEIZMANN INSTITUTE OF SCIENCE



Summary

- **Purpose**
- **CEST-fMRI method design**
- **CEST-fMRI methods**
- **CEST-weighted fMRI results**
- **Towards quantitative CEST-fMRI**
- **Discussion**

Purpose

- BOLD indirectly measures **neurovascular coupling**
 - naturally poor in spatial and temporal resolutions
- Some emerging methods to study brain activation:
 - spectroscopy (fMRS) suggests **metabolic changes**¹
 - diffusion fMRI suggests **structural modifications**²
- **Chemical Exchange Saturation Transfer (CEST)** is sensitive to such metabolic and morphological changes

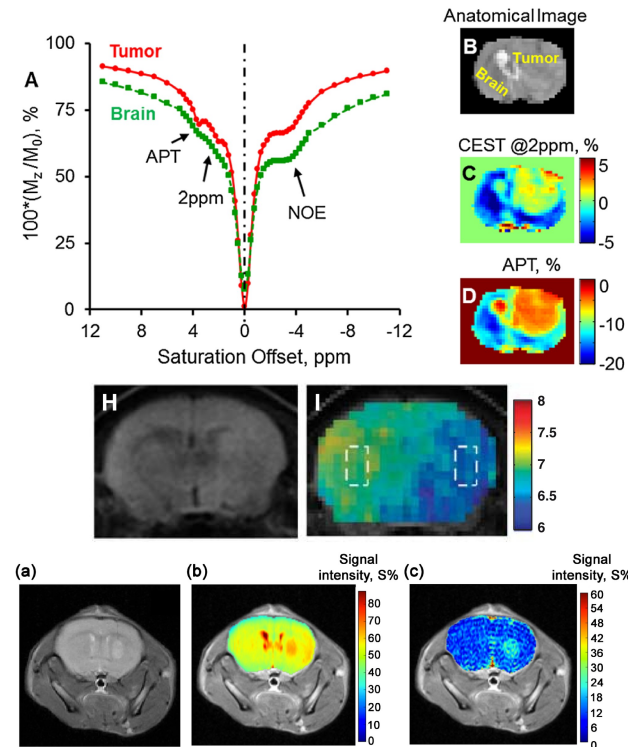
1. Mangia S et al. J Cereb Blood Flow Metab 2009;29:441-463

2. Le Bihan D. Proc Natl Acad Sci U S A. 2006;103:8263-8268

CEST-fMRI method design

→ What is CEST-MRI?

- **Indirect detection of low-concentrated metabolites/proteins/macromolecules** by:
 - Irradiating over small chemical shift ranges
 - Measuring the water signal changes
- Endogenous CEST contrast depends on:
 - Molecule abundance
 - Exchange rates (which can depend on tissue micro-structure and -environment)
 - T1 (which depends on tissue time relaxation properties and B0)
- Applied to brain tumor and stroke imaging



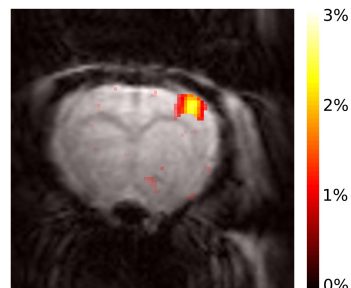
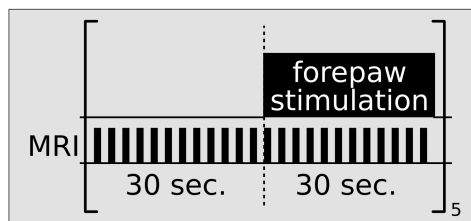
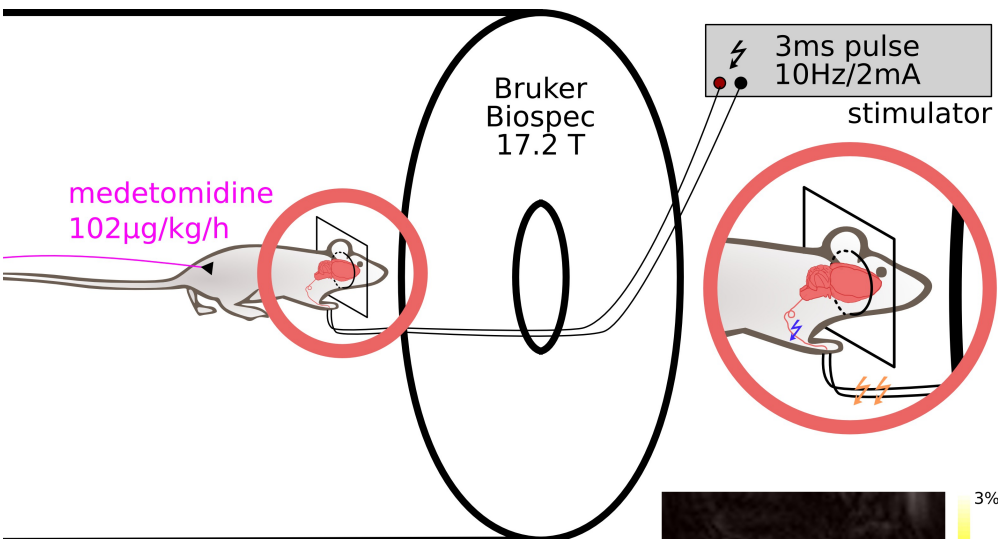
CEST imaging of a 9L glioma in a rat at 9.4T.
Cai K et al. NMR Biomed 2014;28:1-8

CEST pH imaging of a stroke in a rat at 9.4T.
McVicar, N et al. J Cereb Blood Flow Metab 2014;34:690-698

GlucoCEST imaging of a human glioma in a mouse at 11.7T.
Xu X et al. Magn Reson Med 2015;74:1556-1563

CEST-fMRI method design

→ What is fMRI at 17.2T?



BOLD GE-EPI imaging

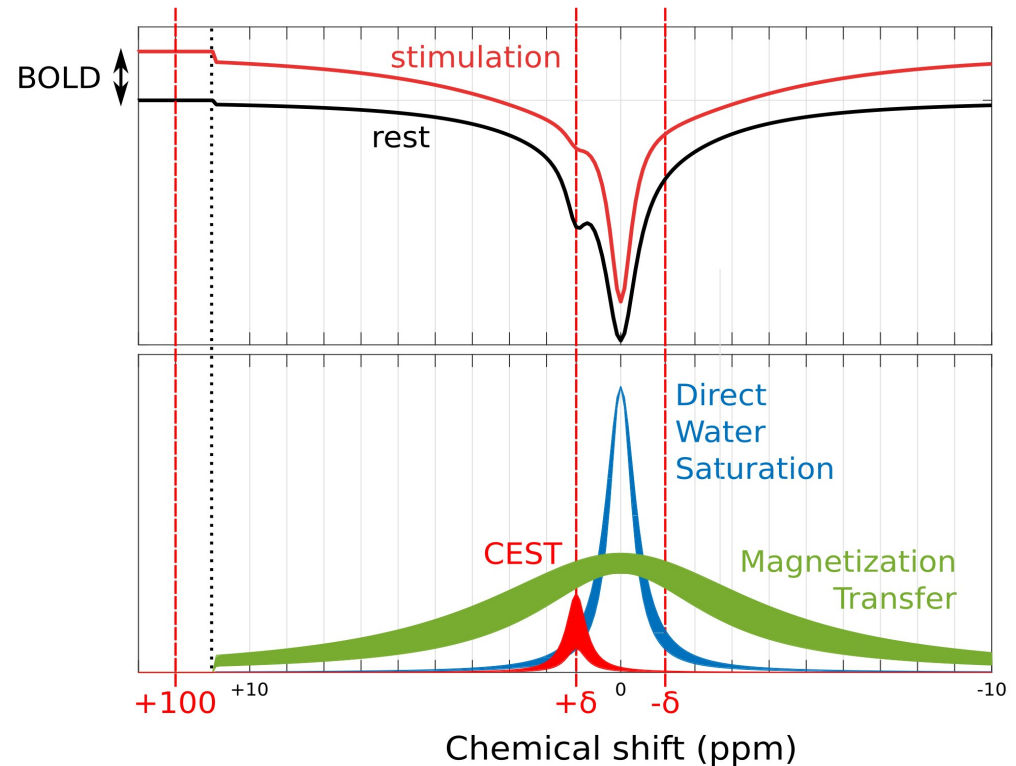
- **Blood-Oxygen-Level Dependent** imaging
- Sprague Dawley rats anesthetized with **medetomidine** (102µg/kg/h)
- Left/right **fore-paw electrical stimulation** (10Hz/2mA)
- **Block-design paradigm** of 10 blocks (30s rest, 30s activation)
- **GE-EPI** (2x2cm FOV, 85x85 matrix, 1.2mm-thick slice, TE/TR=9/2500ms)
- **17.2T** Bruker Biospin, 30-mm diameter surface coil

CEST-fMRI method design

→ Optimization

- General idea: **replace each EPI acquisition by a CEST-EPI scan**
- Problems:
 - **It is CEST!** we need long TRs to perform efficient RF saturation
 - **It is fMRI!** we need short TRs to collect time-domain data and increase sensitivity
 - **BOLD effect!** How to cancel it out?
 - **Magnetization Transfer (MT) effect!**¹ How to cancel it out?

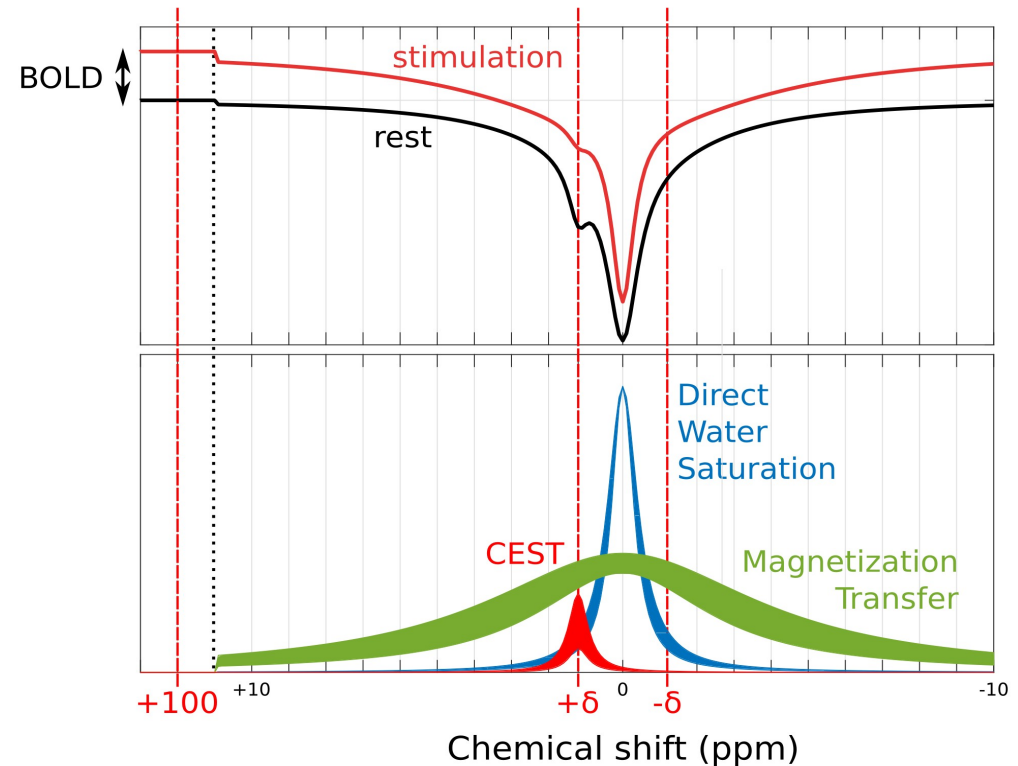
1. Kim T et al. Magn Reson Med. 2008;60:1518-1523



CEST-fMRI method design

→ Optimization

- Question: **How many and which chemical shifts should we irradiate in order to observe a CEST-fMRI contrast free of BOLD and MT effects?**
- Monte Carlo study using simulations of CEST-fMRI signals. Activation consisted in:
 - BOLD effect
 - +1 to +3% broadband intensity change
 - T_2^* changes reflected on the water linewidth
 - $\pm 1\%$ wide-band symmetric MT effect
 - $\pm 0.5\%$ local CEST effect at $+\delta$ ppm
- CEST signals were “acquired” for saturation frequencies $+\delta$, $-\delta$ and $+100$ ppm and mathematically combined

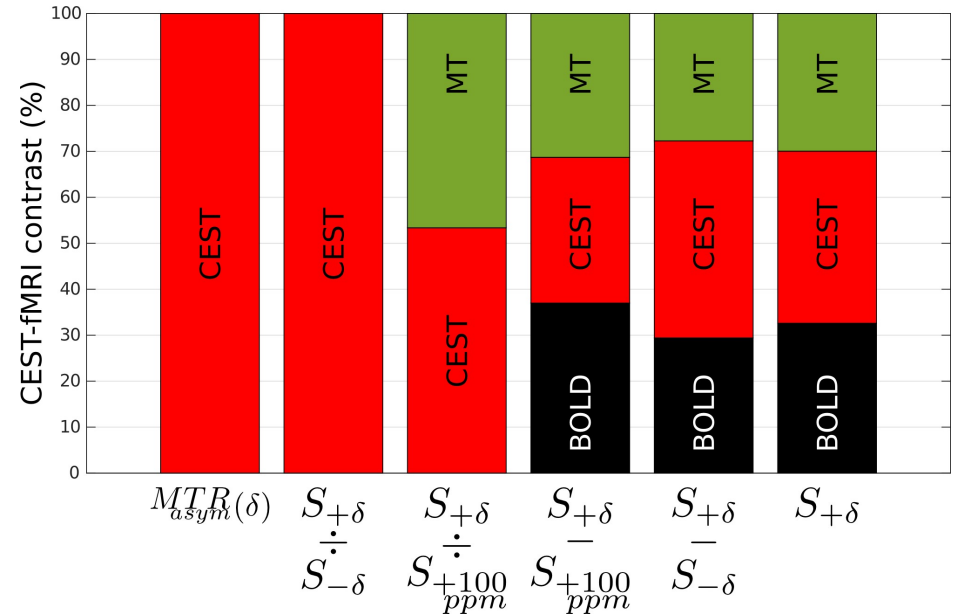


CEST-fMRI experimental design

→ Optimization

Two strategies were selected from the Monte Carlo results:

- **CEST-weighted fMRI strategy**
 - Qualitative CEST measurement
 - 2 saturation freqs: **+ δ and - δ ppm**
 - Processing: ratio of images **$S(+\delta)/S(-\delta)$**
- **Quantitative CEST-fMRI strategy**
 - Based on conventional CEST-MRI
 - 3 saturation freqs: **+ δ , - δ , 100 ppm**
 - Processing: MTR_{asym} map calculation



$$MTR_{asym}(\delta) = \frac{S(-\delta) - S(+\delta)}{S(+100ppm)}$$

CEST-fMRI methods

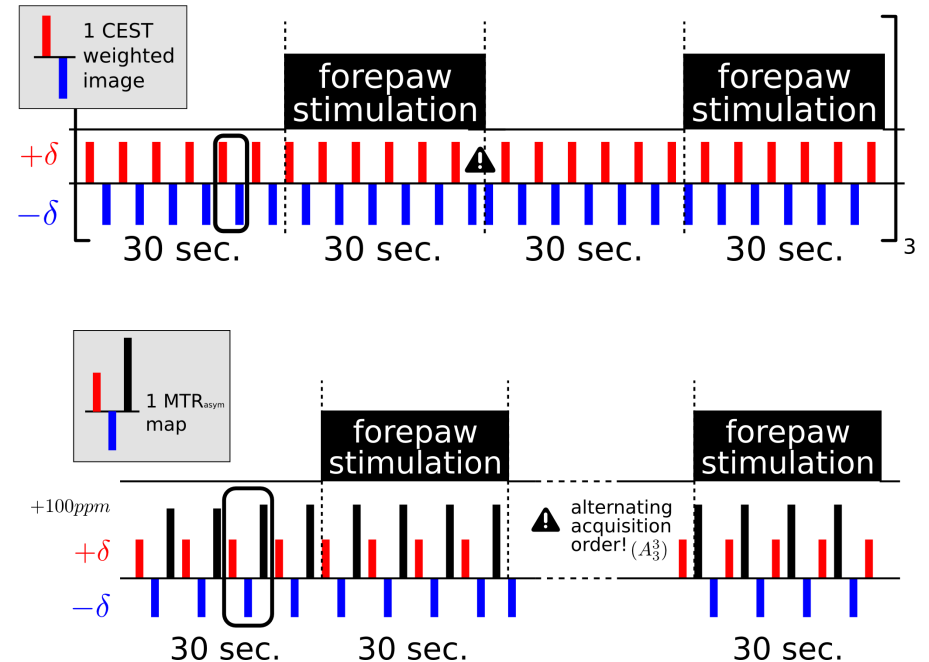
Those two strategies were implemented:

1. CEST-weighted fMRI

- (+) 6 images per block, acceptable time resolution and sensitivity
- (+) Minimum scan time of 2mins
- (-) Qualitative CEST measurement

2. Quantitative CEST-fMRI

- (+) Quantitative CEST measurement
- (-) Minimum scan time of 6mins
- (-) 4 images per block, low time resolution and sensitivity



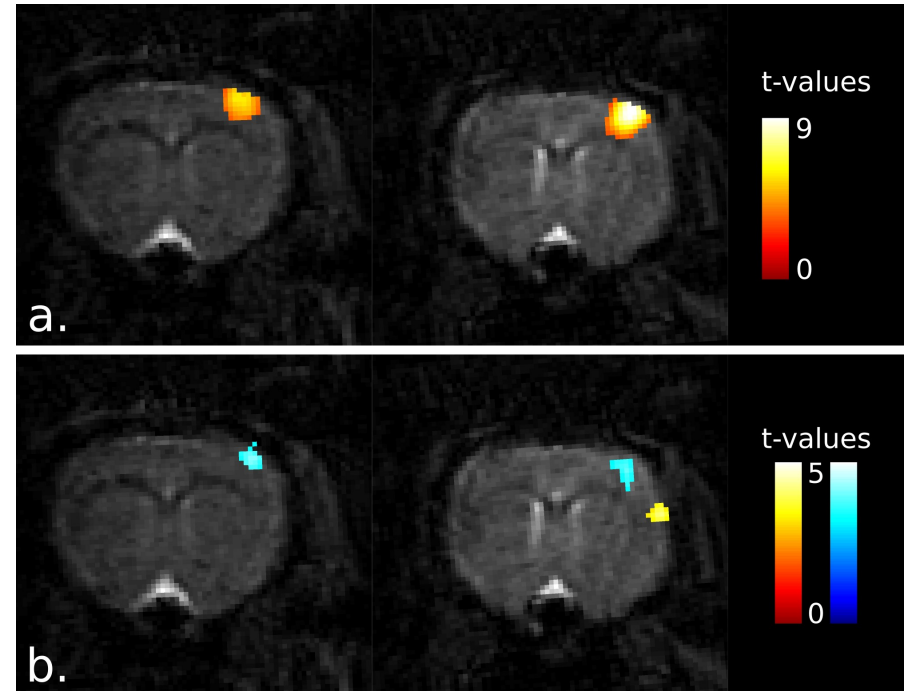
Results: CEST-weighted fMR images

a. BOLD GE-EPI images

b. **CEST-weighted fMR images** acquired with $\delta=1.2\text{ppm}$ (glucose exchange chemical shift).

Image ratios $S(-\delta)/S(+\delta)$ were processed in SPM: intensity drift correction, image registration, SPM fMRI processing and p thresholding (0.001)

- The $S(-\delta)/S(+\delta)$ fMR images show a **spatially localized decrease (blue)**, matching the **BOLD activation area**
- No significant changes were successfully imaged for $\delta=2\text{ppm}$ or $\delta=3.5\text{ppm}$ (APT¹)



1. APT=Amide Proton Transfer, commonly-used CEST-MRI method

Results: CEST-weighted fMRI time courses

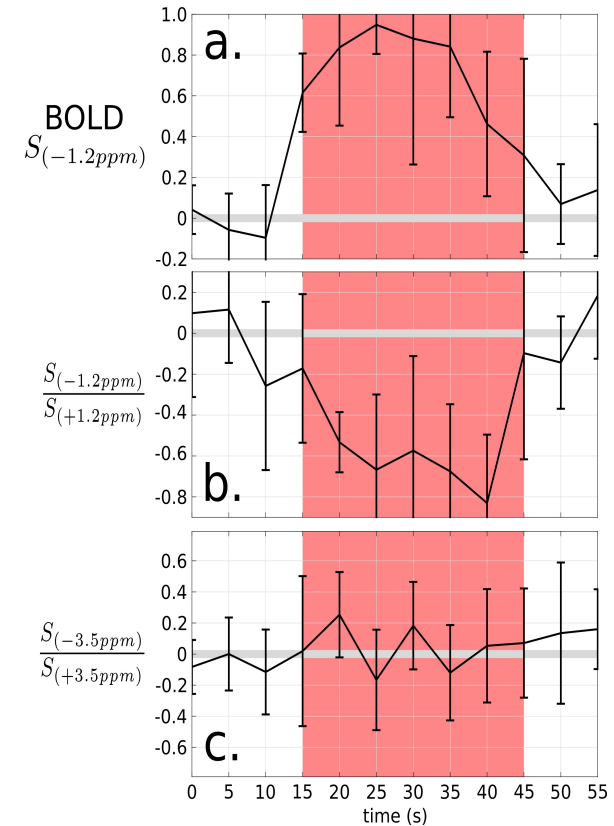
a. **BOLD** time evolution signal

b. **CEST-weighted** time evolution
 $S(-\delta)/S(+\delta)$ with $\delta=1.2\text{ppm}$ (glucose)

c. **CEST-weighted** time evolution
 $S(-\delta)/S(+\delta)$ with $\delta=3.5\text{ppm}$ (APT)

Signals were extracted from the BOLD activation ROI

- **$\delta=1.2\text{ppm}$** : $S(-\delta)/S(+\delta)$ decreases in average of -0.6% during stimulation (n=5 animals, BOLD<0.5% rejected)
- **$\delta=3.5\text{ppm}$** : No significant changes were observed (n=4 animals, BOLD<0.5% rejected)

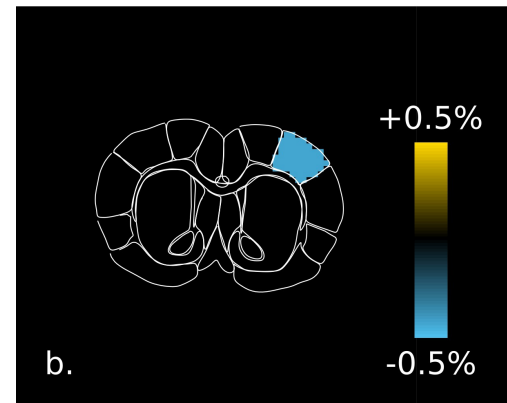
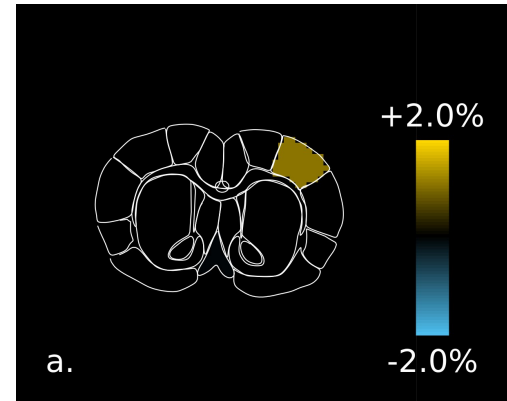


Results: CEST-weighted atlas brain analysis

a. **BOLD** segmented brain atlas
($p < 0.05$)

b. **CEST-weighted** segmented brain
image $S(-\delta)/S(+\delta)$ with $\delta = 1.2\text{ppm}$
($p < 0.05$)

- $n=5$ animals, BOLD $< 0.5\%$ rejected,
1.08mm Bregma rat brain atlas
- An increase in BOLD and a decrease of
the ratio $S(-\delta)/S(+\delta)$ is observable in the
primary somatosensory cortex (S1F)



Towards quantitative CEST-fMRI

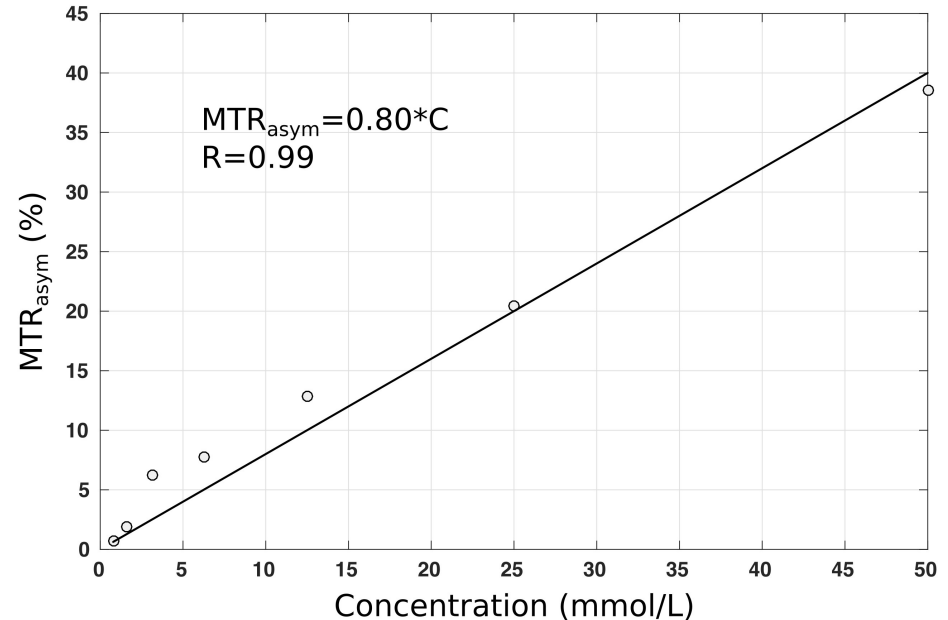
- **Method**

In order to **quantify our observations at $\delta=1.2\text{ppm}$** using the CEST-weighted method, we performed:

- Careful *in vitro* calibrations on glucose samples with 0 to 50 mmol/L concentrations (pH=7.2)
- *In vivo* measurements using the quantitative CEST-fMRI method based on MTR_{asym}

- **Results**

- An **average MTR_{asym} decrease of -0.052%** was observed during stimulation
- According to the *in vitro* calibration, this would correspond to a **glucose concentration decrease of -65 $\mu\text{mol/kg}$** during brain activation



Discussion

- Previous studies using fMRS,^{1,2,3} PET⁴ and PET-MRI⁵ showed an **increased consumption** during brain activation
 - causing a temporary **drop of the glucose concentration**⁶
- Further investigations are needed to estimate the cerebral metabolic rate of glucose (**CMR_{glc}**) using CEST-fMRI data
- A drop in GlucoCEST signal could also originate from a decrease of the **glucose exchange rates** (changes in the micro-environment and/or micro-structure of neurons?)

1. Chen W et al. Proc Natl Acad Sci U S A 1993;90:9896-9900

2. Hyder F et al. J Cereb Blood Flow Metab 1997;17:1040-1047

3. Shestov AA et al. Am J Physiol Endocrinol Metab 2011;301:E1040-1049

4. Fox PT et al. Science 1988;241:462-464

5. Wehrl HF et al. Nat Med 2013;19:1184-1189

6. Giove F et al. Magn Reson Imaging 2003;21:1283-1293

Conclusions

- Some limitations of CEST-fMRI methods:
 - Sensitivity!
 - BOLD and MT effects contamination
 - Sensitive to dynamic water resonance frequency shift (susceptibility)
- Promising results!
- Not limited to glucose: lactate, glutamate, creatine and various proteins involved in the metabolism and the micro-structure of neurones have exchanging properties
- **Potentially a new contrast mechanism for fMRI**
- **Imaging of real-time metabolic changes upon neuronal activation**

Thanks for your attention



- This research was supported by:
 - CEA Enhanced Eurotalents
 - The Louis-Jeantet Foundation
 - The French National Research Agency (ANR-13-NEUC-0002-01)
- Many thanks to:
 - Boucif Djemai
 - Tom Tsurugizawa

